Optimal mass transport as a distance measure between images

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Acknowledgements

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[1] J. Karlsson, and A. Ringh. Generalized Sinkhorn iterations for regularizing inverse problems using optimal mass transport. *SIAM Journal on Imaging Sciences*, 10(4), 1935-1962, 2017.

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Code: https://github.com/aringh/Generalized-Sinkhorn-and-tomography The code is based on ODL: https://github.com/odlgroup/odl

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Outline

- Background
 - Inverse problems
 - Optimal mass transport
 - Sinkhorn iterations solving discretized optimal transport problems
- Sinkhorn iterations as dual coordinate ascent
- Inverse problems with optimal mass transport priors
- Example in computerized tomography



Consider the problem of recovering $f \in X$ from data $g \in Y$, given by

g = A(f) +'noise'

Notation:

- X is called the reconstruction space.
- Y is called the data space.
- $A: X \to Y$ is the forward operator.
- $A^*: Y \to X$ denotes the adjoint operator



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Problems of interest are ill-posed inverse problems:

- a solution might not exist,
- the solution might not be unique,
- the solution does not depend continuously on data.

Simply put: A^{-1} does not exist as a continuous bijection!

Comes down to: find approximate inverse A^{\dagger} so that

$$g = A(f) + \text{'noise'} \implies A^{\dagger}(g) \approx f.$$

A common technique to solve ill-posed inverse problems is to use variational regularization:

 $\argmin_{f \in X} \ \mathcal{G}(A(f),g) + \lambda \mathcal{F}(f)$

- $\mathcal{G}: Y \times Y \to \mathbb{R}$, data discrepancy functional.
- $\mathcal{F}: X \to \mathbb{R}$, regularization functional.
- λ is the regularization parameter. Controls trade-off between data matching and regularization.

Common example in imaging is total variation regularization:

- $G(h,g) = ||h-g||_2^2$,
- $\mathcal{F}(f) = \|\nabla f\|_1$.

If A is linear this is a convex problem!

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One way: consider

$$rgmin_{f\in X} \mathcal{G}(\mathcal{A}(f), g) + \lambda \mathcal{F}(f) + \gamma \mathcal{H}(\tilde{f}, f)$$

f is prior/template *H* defines "closeness" to *f*.
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- \tilde{f} is prior/template
- \mathcal{H} defines "closeness" to \tilde{f} .
- What is a good choice for \mathcal{H} ?

Scenarios where potentially of interest.

- incomplete measurements, e.g. limited angle tomography.
- spatiotemporal imaging:
 - data is a time-series of data sets: $\{g_t\}_{t=0}^T$.

For each set, the underlying image has undergone a deformation.

• each data set g_t normally "contains less information": $A^{\dagger}(g_t)$ is a poor reconstruction.

Approach: solve coupled inverse problems

$$\argmin_{f_0,...,f_T \in \mathcal{X}} \sum_{j=0}^T \left[\mathcal{G}(\mathcal{A}(f_j),g_j) + \lambda \mathcal{F}(f_j) \right] + \sum_{j=1}^T \gamma \mathcal{H}(f_{j-1},f_j)$$

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One suggestion: measure it pointwise, e.g., using an L_p metric

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Draw-backs: for example unsensitive to shifts.

Example: It gives the same distance from f_0 to f_1 and f_2 : $\|f_0 - f_1\|_1 = \|f_0 - f_2\|_1 = 8.$





Gaspard Monge





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Let $c(x_0, x_1) : X \times X \to \mathbb{R}_+$ describes the cost for transporting a unit mass from location x_0 to x_1 .

Given two functions $f_0, f_1 : X \to \mathbb{R}_+$, find the function $\phi : X \to X$ minimizing the transport cost

$$\int_X c(x,\phi(x))f_0(x)dx$$





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where ϕ is mass preserving map from f_0 to f_1 :

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Leonid Kantorovich

Again, let $c(x_0, x_1)$ denote the cost of transporting a unit mass from the point x_0 to the point x_1 .

Given two functions f_0 , $f_1 : X \to \mathbb{R}_+$, find a transport plan $M : X \times X \to \mathbb{R}_+$, where $M(x_0, x_1)$ is the amount of mass moved between x_0 to x_1 .



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$$\min_{M\geq 0}\int_{X\times X}c(x_0,x_1)M(x_0,x_1)dx_0dx_1$$



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$$\begin{split} \min_{M\geq 0} \int_{X\times X} c(x_0,x_1) \mathcal{M}(x_0,x_1) dx_0 dx_1 \\ \text{s.t.} \ \ f_0(x_0) &= \int_X \mathcal{M}(x_0,x_1) dx_1, \ x_0 \in X \\ f_1(x_1) &= \int_X \mathcal{M}(x_0,x_1) dx_0, \ x_1 \in X. \end{split}$$



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Background

Measuring distances between functions: optimal mass transport

Define a distance between two functions $f_0(x)$ and $f_1(x)$ using optimal transport

$$T(f_0, f_1) := \begin{cases} \min_{M \ge 0} & \int_{X \times X} c(x_0, x_1) M(x_0, x_1) dx_0 dx_1 \\ \text{s.t.} & f_0(x_0) = \int_X M(x_0, x_1) dx_1, \ x_0 \in X \\ & f_1(x_1) = \int_X M(x_0, x_1) dx_0, \ x_1 \in X. \end{cases}$$

If d(x, y) metric on X and $c(x, y) = d(x, y)^p$, then $T(f_0, f_1)^{1/p}$ is a metric on the space of measures.

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Example revisited: let $c(x, y) = ||x - y||_2^2$

 $T(f_0, f_1) = 4 \cdot (\sqrt{2})^2 = 8,$ $T(f_0, f_2) = 4 \cdot 5^2 = 100$



This indicates that optimal transport is a more natural distance between two images than L_{ρ} , at least if one is a deformation of the other.

A linear programming problem: for vectors $f_0 \in \mathbb{R}^n$ and $f_1 \in \mathbb{R}^m$ and a cost matrix $C = [c_{ij}] \in \mathbb{R}^{n \times m}$, where c_{ij} defines the transportation cost between pixels x_i and x_j , find the transportation plan $M = [m_{ij}] \in \mathbb{R}^{n \times m}$, m_{ij} is the mass transported between pixels x_i and x_j , such that

$$\begin{split} \min_{m_{ij} \geq 0} \sum_{i=1}^{n} \sum_{j=1}^{m} c_{ij} m_{ij} \\ \text{subject to} \quad \sum_{j=1}^{m} m_{ij} = f_0(i), \ i = 1, \dots, n \\ \sum_{i=1}^{n} m_{ij} = f_1(j), \ j = 1, \dots, m \end{split}$$

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$$\min_{M \ge 0} \operatorname{trace}(C^T M)$$

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$$\operatorname{subject to} M \mathbf{1}_m = f_0$$

$$M^T \mathbf{1}_n = f_1$$

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subject to
$$\sum_{j=1}^{m} m_{ij} = f_0(i), \ i = 1, \dots, n \qquad \Longleftrightarrow \qquad \begin{array}{c} \min_{\substack{M \ge 0}} & \operatorname{trace}(C^T M) \\ \text{subject to} & M \mathbf{1}_m = f_0 \\ M^T \mathbf{1}_n = f_1 \\ \sum_{i=1}^{n} m_{ij} = f_1(j), \ j = 1, \dots, m \end{array}$$

Number of variables is $n \cdot m$. To compare the distance between to images of size $n = m = 256 \times 256$: $M \in \mathbb{R}^{256^2 \times 256^2} \implies \text{approximately } 4 \cdot 10^9 \text{variables. Prohibitively large!}$

Solution: introduce an entropy barrier/regularization term $D(M) = \sum_{i,j} (m_{ij} \log(m_{ij}) - m_{ij} + 1)$ [1],

$$T_{\epsilon}(f_0, f_1) := \min_{\substack{M \ge 0}} \operatorname{trace}(C^T M) + \epsilon D(M)$$

subject to $f_0 = M \mathbf{1}$
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• Using Lagrangian relaxation gives

$$L(M, \lambda_0, \lambda_1) = \operatorname{trace}(C^{\mathsf{T}}M) + \epsilon D(M) + \lambda_0^{\mathsf{T}}(f_0 - M\mathbf{1}) + \lambda_1^{\mathsf{T}}(f_1 - M^{\mathsf{T}}\mathbf{1}).$$

M. Cuturi. Sinkhorn distances: Lightspeed computation of optimal transport. In Advances in Neural Information Processing Systems, pages 2292–2300, 2013.

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• Given dual variables λ_0, λ_1 , the minimum m_{ij} is

$$0 = \frac{\partial L(M, \lambda_0, \lambda_1)}{\partial m_{ij}} = c_{ij} + \epsilon \log(m_{ij}) - \lambda_0(i) - \lambda_1(j)$$

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• Expressed as $m_{ij} = e^{\lambda_0(i)/\epsilon} e^{-c_{ij}/\epsilon} e^{\lambda_1(j)/\epsilon}$ $M = \text{diag}(e^{\lambda_0^T/\epsilon}) K \text{diag}(e^{\lambda_1/\epsilon})$

where $K = \exp(-C/\epsilon)$. Here and in what follows $\exp(\cdot)$, $\log(\cdot)$, ./, \odot denotes the elementwise function.

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Original problem too computationally demanding.

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The solution $M = \text{diag}(e^{\lambda_0^T/\epsilon}) K \text{diag}(e^{\lambda_1/\epsilon})$ is specified by n + m unknowns!

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Let $u_0 = \exp(\lambda_0/\epsilon)$, $u_1 = \exp(\lambda_1/\epsilon)$. The optimal solution $M = \operatorname{diag}(u_0)K\operatorname{diag}(u_1)$ needs to satisfy $\operatorname{diag}(u_0)K\operatorname{diag}(u_1)\mathbf{1} = f_0$ and $\operatorname{diag}(u_1)K^T\operatorname{diag}(u_0)\mathbf{1} = f_1$.

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Theorem (Sinkhorn iterations [2])

For any matrix K with positive elements there are diagonal matrices $diag(u_0)$, $diag(u_1)$ such that $M = diag(u_0)Kdiag(u_1)$ has prescribed row- and column-sums f_0 and f_1 . The vectors u_0 and u_1 can be obtained by alternating marginalization:

$$u_0 = f_0./(Ku_1)$$

 $u_1 = f_1./(K^T u_0)$

- Each iteration only requires the multiplications Ku_1 and K^Tu_0 . This is the bottle neck.
- Linear convergence rate.

Thus highly computationally efficient, allowing for solving large problems.

R. Sinkhorn. Diagonal equivalence to matrices with prescribed row and column sums. The American Mathematical Monthly, 74(4), 402–405, 1967.

Several ways to motivate Sinkhorn iterations [1]

- Diagonal matrix scaling
- Bregman projections
- Dykstra's algorithm

 J.D. Benamou, G. Carlier, M. Cuturi, L. Nenna, and G. Peyré. Iterative Bregman projections for regularized transportation problems. SIAM Journal on Scientific Computing, 37(2), A1111-A1138, 2015.

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Here we will introduce yet another interpretation:

- Use a dual formulation
- The Sinkhorn iteration corresponds to dual coordinate ascent
- This allows us to generalize Sinkhorn iterations
- Approach for addressing inverse problem with optimal transport term
- J.D. Benamou, G. Carlier, M. Cuturi, L. Nenna, and G. Peyré. Iterative Bregman projections for regularized transportation problems. SIAM Journal on Scientific Computing, 37(2), A1111-A1138, 2015.

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Sinkhorn iterations as dual coordinate ascent

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• The Lagrangian dual function:

$$\begin{aligned} \varphi(u_0, u_1) &:= \min_{M \ge 0} L(M, u_0, u_1) = L(M^*, u_0, u_1) = \dots \\ &= \epsilon \log(u_0)^T f_0 + \epsilon \log(u_1)^T f_1 - \epsilon u_0^T K u_1 + \epsilon nm. \end{aligned}$$

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• The dual problem is thus

$$\max_{u_0,u_1} \varphi(u_0,u_1)$$

• Taking the gradient w.r.t u_0 and putting it equal to zero gives

$$0=f_0./u_0-Ku_1,$$

and w.r.t u_1 gives

$$0=f_{1}./u_{1}-\left(u_{0}^{T}K\right)^{T}.$$

These are the Sinkhorn iterations!

For g proper, convex and lower semicontinuous, we can now consider problems of the form

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Can be solve by dual coordinate ascent

$$egin{aligned} u_0 &= f_0./(\mathcal{K} u_1) \ 0 &\in \partial g^*(-\epsilon \log(u_1)) rac{1}{u_1} - \mathcal{K}^{ op} u_0, \end{aligned}$$

if the second inclusion can be solved efficiently.

Can be solvable when $\partial g^*(\cdot)$ is component-wise. Example of such cases:

• $g(\cdot) = \mathcal{I}_{\tilde{f}}(\cdot)$ indicator function on $\{\tilde{f}\} \rightsquigarrow$ original optimal transport problem • $g(\cdot) = \|\cdot\|_2^2$ Consider the inverse problems

 $\min_{\substack{\mathbf{f}_1 \geq 0}} \|\nabla \mathbf{f}_1\|_1$ subject to $\|A\mathbf{f}_1 - g\|_2 \leq \kappa.$

- TV-regularization term: $\|\nabla f_1\|_1$
- Forward model A, data g, and data mismatch term: $||Af_1 g||_2$

Consider the inverse problems

$$\begin{split} \min_{\substack{f_1 \geq 0}} & \|\nabla f_1\|_1 + ``f_1 \text{ close to } f_0'' \\ \text{subject to } & \|Af_1 - g\|_2 \leq \kappa. \end{split}$$

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• Prior fo

Inverse problems with optimal mass transport priors

Consider the inverse problems

$$\begin{split} \min_{\substack{\mathbf{f}_1 \geq 0}} & \|\nabla \mathbf{f}_1\|_1 + \gamma \, \mathcal{T}_\epsilon(\mathbf{f}_0, \mathbf{f}_1) \\ \text{subject to} & \|A\mathbf{f}_1 - \mathbf{g}\|_2 \leq \kappa. \end{split}$$

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Large convex optimization problem with several terms, variable splitting common: ADMM, primal-dual hybrid gradient algorithm, primal-dual Douglas-Rachford algorithm.

Common tool in these algorithms: the proximal operator of the involved functions \mathcal{F} .

$$\operatorname{Prox}_{\mathcal{F}}^{\sigma}(h) = \operatorname{argmin}_{f} \mathcal{F}(f) + \frac{1}{2\sigma} \|f - h\|_{2}^{2}.$$

[1] R.T. Rockafellar. Monotone operators and the proximal point algorithm. SIAM Journal on Control and Optimization, 14(5), 877-898, 1976.

Inverse problems with optimal mass transport priors Generalized Sinkhorn iterations

We want to compute the proximal of $T_{\epsilon}(f_0, \cdot)$, given by $\operatorname{Prox}_{T_{\epsilon}(f_0, \cdot)}^{\sigma}(h) = \operatorname{argmin}_{f_1} T_{\epsilon}(f_0, f_1) + \frac{1}{2\sigma} \|f_1 - h\|_2^2.$ Thus we want to solve $\min_{\substack{M \ge 0, f_1}} \operatorname{trace}(C^T M) + \epsilon D(M) + \frac{1}{2\sigma} \|f_1 - h\|_2^2$ subject to $f_0 = M\mathbf{1}$ $f_1 = M^T \mathbf{1}.$ We want to compute the proximal of $T_{\epsilon}(f_0, \cdot)$, given by $\operatorname{Prox}_{T_{\epsilon}(f_{0},\cdot)}^{\sigma}(h) = \operatorname{argmin}_{\epsilon} T_{\epsilon}(f_{0},f_{1}) + \frac{1}{2\pi} \|f_{1} - h\|_{2}^{2}.$ Thus we want to solve $\min_{M \ge 0, f_1} \operatorname{trace}(C^{\mathsf{T}}M) + \epsilon D(M) + \frac{1}{2\epsilon} \|f_1 - h\|_2^2$ subject to $f_0 = M\mathbf{1}$ $f_1 = M^T \mathbf{1}$ Compare to Using dual coordinate ascent, with $g(\cdot) = \frac{1}{2\sigma} \|\cdot -h\|_2^2$, $u_0 = f_0./(Ku_1)$ we get the algorithm: 2 $u_1 = f_1 / (K^T u_0)$ $u_0 = f_0./(Ku_1)$ 2 $u_1 = \exp\left(\frac{h}{2\pi} - \omega\left(\frac{h}{2\pi} + \log\left(K^T u_0\right)\right) + \log(\sigma\epsilon)\right)$

- Here ω denotes the (elementwise) Wright omega function, i.e., $x = \log(\omega(x)) + \omega(x)$.
- Solved elementwise. Bottleneck is still computation of Ku_1 , K^Tu_0 .

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• Solved elementwise. Bottleneck is still computation of Ku_1 , K^Tu_0 .

Theorem

The algorithm is globally convergent, and with linear convergence rate.

Computerized Tomography (CT): imaging modality used in many areas, e.g., medicine.

- The object is probed with X-rays.
- Different materials attenuates X-rays differently \implies incoming and outgoing intensities gives information about the object.
- Simplest model

$$\int_{L_{r,\theta}} f(x) dx = \log\left(\frac{I_0}{I}\right),$$

- f(x) is the attenuation in the point x, which is what we want to reconstruct,
- $L_{r,\theta}$ is the line along which the X-ray beam travels,
- *I*₀ and *I* are the the incoming and outgoing intensities.



Parallel beam 2D CT example:

- Reconstruction space: 256×256 pixels
- Angles: 30 in $[\pi/4, 3\pi/4]$ (limited angle)
- Detector partition: uniform 350 bins
- Noise level 5%



TV-regularization and ℓ_2^2 prior: $\min_{f_1} \gamma \|f_0 - f_1\|_2^2 + \|\nabla f_1\|_1$ subject to $\|Af_1 - w\|_2 \le \kappa$. TV-regularization and optimal transport prior: $\min_{f_1} \gamma T_{\epsilon}(f_0, f_1) + \|\nabla f_1\|_1$ subject to $\|Af_1 - w\|_2 \le \kappa$.





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Comparing different regularization parameters for the problem with ℓ_2^2 prior.

$$\begin{split} \min_{f_1} & \gamma \|f_0 - f_1\|_2^2 + \|\nabla f_1\|_1 \\ \text{subject to} & \|Af_1 - w\|_2 \leq \kappa. \end{split}$$



Figure: Reconstructions using ℓ_2 prior with different regularization parameters γ .

Parallel beam 2D CT example:

- Reconstruction space: 256×256 pixels
- Angles: 30 in [0, π]
- Detector partition: uniform 350 bins
- Noise level 3%



Parallel beam 2D CT example:

- Reconstruction space: 256×256 pixels
- Angles: 30 in $[0, \pi]$
- Detector partition: uniform 350 bins

Noise level 3%

15

10 >

> -5 -10

-15 -



Conclusions

- Optimal mass transport a viable framework for imaging applications
- Generalized Sinkhorn iteration for computing the proximal operator of optimal transport cost
- Use variable splitting for solving the inverse problem
- Application to CT reconstruction using optimal transport priors

Conclusions

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Potential future directions:

• Application to spatiotemporal image reconstruction:

$$\argmin_{f_0,...,f_T \in \mathcal{X}} \sum_{j=0}^T \left[\mathcal{G}(\mathcal{A}(f_j),g_j) + \lambda \mathcal{F}(f_j) \right] + \sum_{j=1}^T \gamma \mathcal{H}(f_{j-1},f_j)$$

- More efficient ways of solving the dual problem?
- Learning for inverse problems using optimal transport as a loss function

Questions?